

# Multi-Label Transduction for Identifying Disease Comorbidity Patterns

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**Abstract.** Study of the untoward effects associated with the comorbidity of multiple diseases on brain morphology requires identifying differences across multiple diagnostic groupings. To identify such effects and differentiate between groups of patients and normal subjects, conventional methods often compare each patient group with healthy subjects using binary or multi-class classifiers. However, testing inferences across multiple diagnostic groupings of complex disorders commonly yield inconclusive or conflicting findings when the classifier is confined to modeling two cohorts at a time or considers class labels mutually-exclusive (as in multi-class classifiers). These shortcomings are potentially caused by the difficulties associated with modeling compounding factors of diseases with these approaches. Multi-label classifiers, on the other hand, can appropriately model disease comorbidity, as each subject can be assigned to two or more labels. In this paper, we propose a multi-label transductive (MLT) method based on low-rank matrix completion that is able not only to classify the data into multiple labels but also to identify patterns from MRI data unique to each cohort. To evaluate the method, we use a dataset containing individuals with Alcohol Use Disorder (AUD) and human immunodeficiency virus (HIV) infection (specifically 244 healthy controls, 227 AUD, 70 HIV, and 61 AUD+HIV). On this dataset, our proposed method is more accurate in correctly labeling subjects than common approaches. Furthermore, our method identifies patterns specific to each disease and AUD+HIV comorbidity that shows that the comorbidity is characterized by a compounding effect of AUD and HIV infection.

## 1 Introduction

Improvements in modern health-care together with the aging population caused populations with multiple conditions that require ongoing medical attention. The U.S. alone has approximately 75 million people living with 2 or more conditions [12] such as brain-related disorders. For brain-related conditions, disease comorbidity often leads to new cognitive impairments [8,9]. However, few studies have examined the potentially heightened burden of disease comorbidity. As an example, Alcohol Use Disorder (AUD) is common among individuals in the United States, and its co-occurrence in individuals with human immunodeficiency virus (HIV) infection is high [8], occurring at twice the rate as occurs in the

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general population [9]. Both AUD and HIV infection reduce health-related quality of life. Adapting robust and multi-label technology can transform the mechanistic understanding of the compounding factors of such comorbidity.

Conventional models for identifying the compounding effects of disease comorbidity use binary (such as statistical tests [9]) or multi-class (*e.g.*, [15,12]) study designs. By nature, these methods assume samples are assigned to mutually-exclusive labels, and hence inaccurately model the compounding factors of disease comorbidity. Thus, they often lead to inconclusive or contradicting findings for the cases of comorbidity [14,16]. One can accurately model disease comorbidity by allowing multiple labels to be assigned to each subject, such as done by multi-label classification methods. However, there are two major challenges in applying multi-label methods to neuroimaging data: (1) neuroimaging data often contain several brain morphology measures that are highly correlated; (2) the measures are prone to noise due to inaccuracies in acquisition, preprocessing, and diagnosis of subjects. To overcome these challenges, we introduce a multi-label transductive (MLT) classification approach based on low-rank matrix completion (MC) [7,2] that models noise and overcomes the problem of feature redundancy/correlation by reducing the data to low-rank subspaces. In addition, our method identifies patterns related to each disease (label).

To gain a better understanding of MLT, consider a training data set of  $N_{tr}$  samples with  $l$  different labels (which lead to  $c = 2^l$  number of different classes). Let  $d$  be the dimensionality of the feature space,  $N = N_{tr} + N_{ts}$  the number of total samples ( $N_{ts}$  the number of testing samples). Our MLT then determines the labels of the testing samples by first combining all features (of training and testing) and the labels of the training data into a matrix. Here, we propose to add columns to the matrix, in which only the labels but not the features are defined. These allow us to compute disease specific patterns, which, together with the testing labels are computed by MLT through matrix completion.

We apply our model to identify the impact of alcohol use and HIV infection in the brain morphometry of individuals. We interpret the two conditions AUD and HIV as labels that encode four classes: CTRL (samples are assigned to none of the two labels), AUD (only assigned to the first label), HIV (only assigned to the second label), and AUD+HIV (having both labels). Fig. 1 shows the corresponding matrix whose missing values are computed by our method (see<sup>1</sup> for notations).

In summary, we make two contributions: we model disease comorbidity within a transductive multi-label setting that is robust to noise, and we identify the disease-specific patterns by modifying the original MC algorithm [7].

## 2 Multi-Label Transduction via Matrix Completion

MC is the process of recovering a matrix from a sampling of its entries. Specifically, MC recovers a data matrix  $\mathbf{D}$  from a matrix  $\mathbf{D}^0$  for which only the subset  $\Omega$

<sup>1</sup> Bold capital letters denote matrices (*e.g.*,  $\mathbf{D}$ ), and bold small letters denote vectors (*e.g.*,  $\mathbf{d}$ ). All non-bold letters are scalar variables.  $d_{ij}$  is the scalar in row  $i$  and column  $j$  of  $\mathbf{D}$ .  $|A|$  denotes the number of elements in set  $A$ .  $\|\mathbf{D}\|_*$  designates the nuclear norm (sum of singular values) of  $\mathbf{D}$ .

	Training Labels				Testing Labels				CTRL	AUD	HIV	AUD+HIV
AUD	$y_{11}$	$y_{12}$	$\dots$	$y_{1N_{tr}}$	?	$\dots$	?	-1	+1	-1	+1	
HIV	$y_{21}$	$y_{22}$	$\dots$	$y_{2N_{tr}}$	?	$\dots$	?	-1	-1	+1	+1	
	$x_{11}$	$x_{12}$	$\dots$	$x_{1N_{tr}}$	$x_{1(N_{tr}+1)}$	$\dots$	$x_{1(N_{tr}+N_{ts})}$	?	?	?	?	
	$x_{21}$	$x_{22}$	$\dots$	$x_{2N_{tr}}$	$x_{2(N_{tr}+1)}$	$\dots$	$x_{2(N_{tr}+N_{ts})}$	?	?	?	?	
	$\vdots$	$\vdots$	$\ddots$	$\vdots$	$\vdots$	$\ddots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	$\vdots$	
	$x_{d1}$	$x_{d2}$	$\dots$	$x_{dN_{tr}}$	$x_{d(N_{tr}+1)}$	$\dots$	$x_{d(N_{tr}+N_{ts})}$	?	?	?	?	
	Training Features				Testing Features				Patterns			

Fig. 1: Multi-label transduction (MLT) via matrix completion: each column represents one sample, the top rows hold the labels (two labels in this example, *i.e.*, AUD and HIV), while the rest are comprised of the features. The last columns include the representative features for each of the classes.

of its entries are defined (or observed). Knowing a sufficiently large number of measurements in the matrix, MC assumes that the relation between the elements of the matrix can be accurately described by a low-rank matrix [3,7,2]. Thus, MC estimates the missing entries in  $\mathbf{D}$  by minimizing its rank ( $\text{rank}(\mathbf{D})$ ) while  $d_{ij} = d_{ij}^0, \forall (i, j) \in \Omega$ . The rank function is a non-convex, non-smooth function that can be approximated by the nuclear norm of the matrix, *i.e.*, the sum of its non-vanishing singular values,  $\sigma_k$ :  $\|\mathbf{D}\|_* = \sum_{k=1}^d \sigma_k(\mathbf{D})$ .

To apply MC to classification, we note that classifiers generally learn the relation between the features,  $\mathbf{X}_{tr} \in \mathbb{R}^{d \times N_{tr}}$ , and the labels,  $\mathbf{Y}_{tr} \in \mathbb{R}^{l \times N_{tr}}$ , of the training samples. Learning this relation while at the same time classifying or determining the labels  $\mathbf{Y}_{ts} \in \mathbb{R}^{l \times N_{ts}}$  of the  $N_{ts}$  testing samples (*i.e.*,  $\mathbf{X}_{ts} \in \mathbb{R}^{d \times N_{ts}}$ ) can again be interpreted as a Matrix Completion task [7] of a matrix that contains all training and testing data (see also Fig. 1). MC assumption about rank deficiency of the matrix is equivalent to assuming a linear relationship between the measurements and labels, which is a common assumption of classifiers. However, unlike inductive methods that learn a separate model and then apply it to testing data, MC classifies the testing samples by filling in the submatrix  $\mathbf{Y}_{ts}$  of missing entries such that rank of the matrix is minimized. As discussed earlier (and illustrated in Fig. 1), we propose to extract class-specific patterns by adding columns (*i.e.*, submatrices  $\mathbf{Y}_{pat} \in \mathbb{R}^{l \times c}$  and  $\mathbf{X}_{pat} \in \mathbb{R}^{d \times c}$ ) with empty entries for the features to the matrix. As in [7,2], a row with the entries of all 1 (called ‘1’ row) is added to the matrix modeling the bias term of linear classifiers (see Eq. (1)). In summary,  $\mathbf{D}^0$  is formed by concatenating all features ( $\mathbf{X}_{tr}$ ,  $\mathbf{X}_{ts}$ ,  $\mathbf{X}_{pat}$ ), labels ( $\mathbf{Y}_{tr}$ ,  $\mathbf{Y}_{ts}$ ,  $\mathbf{Y}_{pat}$ ), and the ‘1’ row.

The set of known entries in  $\mathbf{D}^0$  is now defined by the ‘feature’ submatrix  $\Omega_X$  (*i.e.*, all training  $\mathbf{X}_{tr}$  and testing  $\mathbf{X}_{ts}$  features) and the label submatrix  $\Omega_Y$  (*i.e.*, all training labels  $\mathbf{Y}_{tr}$  and the pattern-specific labels  $\mathbf{Y}_{pat}$ ). Note, that the extracted neuroimaging measurements (used as features) may be contaminated by noise due to inaccuracies in acquisition or preprocessing. In addition, the brain

of a patient might not yet be impacted by a disease so that the patient looks more like a sample from the control cohort. This variability within cohorts can also be interpreted as noise associated with the training labels. We model those sources of noise in our MC approach by introducing the matrix  $\mathbf{E}$  and defining  $\mathbf{D}$  as sum between  $\mathbf{D}^0$  and  $\mathbf{E}$ :

$$\mathbf{D} = \begin{bmatrix} \mathbf{D}_Y \\ \mathbf{D}_X \\ \mathbf{D}_1 \end{bmatrix} = \begin{bmatrix} \mathbf{Y}_{tr} & \mathbf{Y}_{ts} & \mathbf{Y}_{pat} \\ \mathbf{X}_{tr} & \mathbf{X}_{ts} & \mathbf{X}_{pat} \\ \mathbf{1}^\top & & \end{bmatrix} + \begin{bmatrix} \mathbf{E}_{Y_{tr}} & \mathbf{0} & \mathbf{0} \\ \mathbf{E}_{X_{tr}} & \mathbf{E}_{X_{ts}} & \mathbf{0} \\ \mathbf{0}^\top & & \end{bmatrix} = \mathbf{D}^0 + \mathbf{E}, \quad (1)$$

where  $\mathbf{D}_Y$ ,  $\mathbf{D}_X$ , and  $\mathbf{D}_1$  are the label, feature and ‘1’ rows of  $\mathbf{D}$ , respectively. In other words, MC determines the testing labels  $\mathbf{Y}_{ts}$ , representative patterns for each class  $\mathbf{X}_{pat}$ , and the noise  $\mathbf{E}$  such that the rank of  $\mathbf{D} = \mathbf{D}^0 + \mathbf{E}$ , *i.e.*,  $\|\mathbf{D}\|_*$ , is minimized. To further constrain the optimization problem and avoid trivial solutions, we introduce the squared loss function  $\mathcal{L}_x(d_{ij}, d_{ij}^0) = \frac{1}{2}(d_{ij} - d_{ij}^0)^2$  as a way to penalize large differences in features (*i.e.*, noise in features) between the two matrices and a log loss function  $\mathcal{L}_y(d_{ij}, d_{ij}^0) = \frac{1}{\gamma} \log(1 + e^{-\gamma d_{ij} d_{ij}^0})$  to penalize difference in class assignment between the matrices (*i.e.*, noise in labeling).  $\gamma = 1$  in our experiments. The complete minimization problem is then defined as

$$\underset{\mathbf{D}, \mathbf{E}}{\operatorname{argmin}} \|\mathbf{D}\|_* + \frac{\lambda_1}{|\Omega_X|} \sum_{ij \in \Omega_X} \mathcal{L}_x(d_{ij}, d_{ij}^0) + \frac{\lambda_2}{|\Omega_Y|} \sum_{ij \in \Omega_Y} \omega_{ij} \mathcal{L}_y(d_{ij}, d_{ij}^0) \quad (2)$$

$$\text{subject to } \mathbf{D} = \mathbf{D}^0 + \mathbf{E}, \mathbf{D}_1 = \mathbf{1}^\top,$$

with hyperparameters  $0 \leq \lambda_1, \lambda_2 \leq 1$  controlling the influence of the loss functions in the minimization problem and the weight  $\omega_{ij}$  of each training sample accounting for the imbalance in number of samples per cohort. This weight, computed as a processing step, weights the loss for each sample disproportional to the number of samples available in the training set with the same label  $y_{ij}$  of sample  $j$ .

**Solving the optimization problem.** As in [7,2,1], Eq. (2) is a constrained, convex optimization problem that is not smooth due to the nuclear norm (first term). We estimate its solution via the fixed-point continuation (FPC) [7], one of the interior point methods that can be applied to such problems. FPC iteratively alternates between updating the gradient of the loss terms  $\mathcal{L}_x(\cdot)$  and  $\mathcal{L}_y(\cdot)$ , and the singular value thresholding (SVT) [3], which is used for minimizing the nuclear norm. Cabral *et al.* [2] proved the constrained optimization (similar settings as in Eq. (2)) converges to the optimal solution.

**Identifying Disease Patterns.** As a result of completing the matrix in Eq. (1), the unknown entries in  $\mathbf{X}_{pat}$  are determined. Since MC minimizes the rank of the matrix, it fills the entries in  $\mathbf{X}_{pat}$  such that they have maximum correlations with their respective labels in  $\mathbf{Y}_{pat}$  (*i.e.*,  $(-1, -1)$ ,  $(-1, +1)$ ,  $(+1, -1)$ ,  $(+1, +1)$ ). The columns of  $\mathbf{X}_{pat}$  can, hence, be considered as representative patterns for each class. Since we are interested in identifying how each of these classes are different from the control group, we simply compute the difference between the representative pattern of each class and the CTRL group, *i.e.*,

$$\mathbf{p}^{\text{AUD}} = |\mathbf{x}_{pat}^{\text{CTRL}} - \mathbf{x}_{pat}^{\text{AUD}}|, \mathbf{p}^{\text{HIV}} = |\mathbf{x}_{pat}^{\text{CTRL}} - \mathbf{x}_{pat}^{\text{HIV}}|, \text{ and } \mathbf{p}^{\text{AUD+HIV}} = |\mathbf{x}_{pat}^{\text{CTRL}} - \mathbf{x}_{pat}^{\text{AUD+HIV}}|,$$

where  $\mathbf{p}^c$  denotes the identified pattern for class  $C$ , and  $\mathbf{x}_{pat}^c$  is the corresponding column in  $\mathbf{X}_{pat}$  for class  $C$ . We view small differences as noise and omit them from our findings by introducing the tolerance threshold  $\epsilon$  and discarding the values  $\mathbf{p}^c < \epsilon$  ( $\epsilon = 10^{-3}$  in our experiments).

### 3 Experiments

We now compare the accuracy of the proposed and alternative methods with respect to the multi-label AUD/HIV dataset. Alternative implementations include running MC separately for each label, denoted by Single Label MC (SL-MC) [7], and running our proposed method (similar to [3]) without considering the error matrix  $\mathbf{E}$  (see Eq. (1); denoted as MLT-EMC). The comparison also includes the widely used multi-class SVM (MC-SVM) [4] and multi-label SVM (ML-SVM) [10,4]. For fair comparison, we ran the SVMs by weighing samples (similar to the weights  $\omega_{ij}$  we used in our formulation) in the corresponding cost function according to the size of the associated class.

#### 3.1 Dataset and Preprocessing

As summarized in Table 1, the dataset consists of the morphometric measurements extracted from the magnetic resonance images (MRIs) of 244 healthy controls (CTRL), 227 AUD subjects without HIV infection, 70 HIV-infected individuals that do not meet the criteria for AUD (HIV), and 61

Table 1: Details of the multi-label dataset (‘svol’ = supratentorial volume).

	Total	sex		Age (years)	svol ( $\times 10^6$ )
		F	M		
CTRL	244	122	123	45.59 $\pm$ 17.17	1.27 $\pm$ 0.13
AUD	227	67	159	48.49 $\pm$ 10.04	1.27 $\pm$ 0.11
HIV	70	20	45	51.81 $\pm$ 8.44	1.27 $\pm$ 0.15
AUD+HIV	61	23	43	50.97 $\pm$ 8.12	1.23 $\pm$ 0.14

subjects with both AUD and HIV infection (HIV+AUD). For additional details about data collection and preprocessing, please refer to [13].

We apply the cross-sectional approach of FreeSurfer 5.3.0 software to the skull-stripped T1w MRI of each subject in order to measure the *mean curvature* (*MeanCurv*), *surface area* (*SurfArea*), *gray matter volume* (*GrayVol*), and *average thickness* (*ThickAvg*) of 34 bilateral cortical Regions Of Interest (ROIs), the volumes of 8 bilateral subcortical ROIs (*i.e.*, thalamus, caudate, putamen, pallidum, hippocampus, amygdala, accumbens, cerebellar cortex), the volumes of 5 subregions of the corpus callosum (posterior, mid-posterior, central, mid-central and anterior), the volume of all white matter hypointensities, the left and right lateral and third ventricles, and the supratentorial volume (svol). In addition to svol, each subject is thus represented by the z-scores of 298 morphometric features.

**Confounding Factors.** With respect to the CTRL group, *age*, *sex*, and *svol* significantly impact ( $p$ -value  $< 0.001$ ) the morphometric measurements according to the paired t-test between each demographic factor and feature. To omit their influence from the analysis, we capture the relationship between each feature

and the confounding factors by parameterizing a generalized linear model (GLM) [11] on the CTRL cohort of each training run within the cross-validation. After parameterizing GLM, the model is applied to the measurements of each subject to compute the residual score that are indifferent to the confounding factors. Note, the GLM model is only trained on the data from the training folds not to involve testing data in the preprocessing stage.

**Evaluation.** The classification accuracy of each method is measured via 10-fold nested cross-validation with the hyperparameters determined via 5-fold inner cross-validation. For MLT and SL-MC, the search space of the hyperparameters  $\lambda_1$  and  $\lambda_2$  is  $\{0.001, 0.01, 0.1, 0.5, 0.9, 1\}$ , and for MLT-EMC we do not have those hyperparameters as there is no error terms associated. The setting of FPC hyperparameters are set according to [2]. We also rely on the literature to set the search space for the hyperparameters of the alternative approaches, each based on their respective references, MC-SVM [4] and ML-SVM [10] (*e.g.*, the search space for the hyperparameter  $C$  of SVM is  $\{0.01, 0.1, 1, 10, 100\}$ ).

We summarize the outcome of each approach through several accuracy scores. Specifically, for each class  $C$  with  $P^C$  positive and  $N^C$  negative samples, we compute for each approach the precision (Pre) and recall (Rec) based on the true positive (TP), true negative (TN), false positive (FP) and false negative (FN) of the classifier:  $\text{Pre}^C = \text{TP}^C / (\text{TP}^C + \text{FP}^C)$  and  $\text{Rec}^C = \text{TP}^C / (\text{TP}^C + \text{FN}^C)$ . We also report the area under the ROC curve (AUC) and balanced accuracy (BAc) score for all methods:  $\text{BAc}^C = 1/2 \cdot (\text{TP}^C / P^C + \text{TN}^C / N^C)$ . To evaluate the performance with respect to each separate class, we also use true positive rate (TPR) metric, which shows the portion of subjects identified correctly:  $\text{TPR}^C = \text{TP}^C / P^C$ .

### 3.2 Results and Comparison

Table 2 summarizes the accuracy scores with respect to the two defined labels (*i.e.*, AUD and HIV. BAc scores marked with a ‘†’ are associated with a Fisher’s exact test [6] that was significantly better than chance (*i.e.*,  $p$ -value  $< 0.001$ ). Our

Table 2: Comparison for each single label. † sign indicates a  $p$ -value  $< 0.001$  in a Fisher exact test.

Method	AUD				HIV			
	BAc	Pre	Rec	AUC	BAc	Pre	Rec	AUC
Ours (MLT)	<b>.68†</b>	<b>.67</b>	<b>.69</b>	<b>.69</b>	<b>.78†</b>	<b>.75</b>	.79	<b>.80</b>
SL-MC [7]	.61	.63	.58	.65	.72†	.68	.70	.70
MLT-EMC [3]	.52	.53	.51	.55	.59	.60	.56	.62
MC-SVM [4]	.63	.61	.63	.60	.72†	.68	.74	.70
ML-SVM [10]	.66†	.64	.65	.66	.75†	.69	<b>.80</b>	.74

proposed method obtains better results in terms of both balanced accuracy and AUC compared to all other methods. In comparison with the second best method (ML-SVM), our BAc scores are by at least 2% and our AUC scores by at least 3% better in both experiments. Also, our method obtains a better balance between precision and recall, specially for the highly imbalanced case of HIV. The results confirm our intuition that the multi-label setting is better in modeling the problem compared to the multi-class methods, as both multi-label methods involved in the comparison (MLT and ML-SVM) lead to the best results. Both SL-MC and MC-SVM perform inferior to them in terms of both balanced

accuracy and AUC. Furthermore, MLT-EMC, *i.e.*, the method without the noise term, obtains the worst results.

Table 3 summarizes the TPR with respect to all four classes (CTRL, AUD, HIV, and AUD+HIV) and the overall mean across the four classes. In a four-class classification problem, a TPR higher than 0.25 is considered better than

Table 3: Class specific TPR and overall mean.

Method	CTRL	AUD	HIV	AUD+HIV	Mean
Ours (MLT)	<b>.57</b>	<b>.54</b>	<b>.57</b>	<b>.59</b>	<b>.57</b>
SL-MC [7]	.38	.35	.32	.33	.35
MLT-EMC [3]	.37	.32	.33	.31	.33
MC-SVM [4]	.42	.44	.40	.44	.43
ML-SVM [10]	.55	.51	.52	.56	.54

chance. The scores agree with the findings of Table 2 in that the multi-label methods (*i.e.*, MLT and ML-SVM) lead to the best models. Our proposed method outperforms ML-SVM by 3% with respect to the overall mean TPR.

Fig. 2 shows the identified patterns by our proposed method. These patterns are composed of approximately 20% of the 298 features for AUD, 16% for HIV and 40% for AUD+HIV, with approximately 5% of the features shared among all these cohorts. These identified patterns suggest that AUD and HIV infection are associated with deficits in cortical and subcortical regions, which agrees with the HIV and Alcohol literature [5,8,9,13]. Furthermore, several previous studies have reported cortical thickness and gray matter volume as important markers for AUD and HIV infection [9,13], which agrees with our findings. Subcortical regions, including hippocampus, thalamus and basal ganglia structures (*i.e.*, Caudate, Putamen, Palladium), are reported in the literature to be affected by HIV and AUD [5], which are also found important by our method. Specifically, the primary motor cortex region, and the basal ganglia subcortical structures are shown to be more severely affected as a result of comorbidity of AUD and HIV, compared to each single one of them.

**Discussions.** The identified patterns of AUD+HIV record the largest number of relevant regions, which can document a compounding effect of AUD and HIV. Another interesting finding of our results is that our method avoids underestimating the impact of the disease to a small number of brain regions as commonly done by sparse classifiers. In addition, since our method spans the data matrix to a

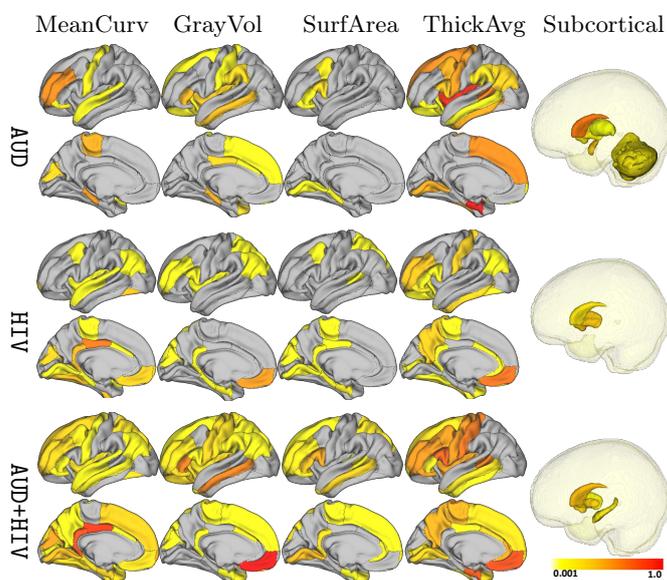


Fig. 2: Identified patterns for AUD, HIV, and AUD+HIV.

low-rank subspace, it can implicitly alleviate the redundancy and correlation among the features that are (linearly) correlated.

## 4 Conclusion

In this paper, we introduced a multi-label transductive classifier that not only classifies the data into multiple labels but also can identify the patterns specific to each disease (labels) and their comorbidity. We experimented on a large set of data with control samples and subjects with alcohol use disorder, HIV infection or both. Our model led to the superior accuracy scores in comparison to state-of-the-art methods. Our method was also able to identify disease-related (and their comorbidity) patterns, which revealed that the comorbidity was characterized by a compounding effect of the two disorders.

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