

# High-Resolution Multishot Diffusion-Weighted Body and Breast MRI using Locally Low-rank regularization

YUXIN HU<sup>1,2</sup>, EVAN G. LEVINE<sup>1,2</sup>, CATHERINE J. MORAN<sup>1</sup>,  
VALENTINA TAVIANI<sup>3</sup>, SHREYAS VASANAWALA<sup>1</sup>, BRUCE L.  
DANIEL<sup>1,4</sup>, AND BRIAN HARGREAVES<sup>1,2,4</sup>

<sup>1</sup>*Department of Radiology, Stanford University, Stanford, CA, United States*

<sup>2</sup>*Department of Electrical Engineering, Stanford University, Stanford, CA, United States*

<sup>3</sup>*GE Healthcare, Menlo Park, CA, United States*

<sup>4</sup>*Department of Bioengineering, Stanford University, Stanford, CA, United States*



JOINT ANNUAL MEETING  
ISMRM–ESMRMB  
16–21 June 2018

SMRT 27<sup>th</sup> Annual Meeting 15–18 June 2018  
[www.smrt.org](http://www.smrt.org)

Paris Expo Porte de Versailles  
Paris, France

# Declaration of Financial Interests or Relationships

Speaker Name: Yuxin Hu

I have the following financial interest or relationship to disclose with regard to the subject matter of this presentation:

Company Name: GE Healthcare

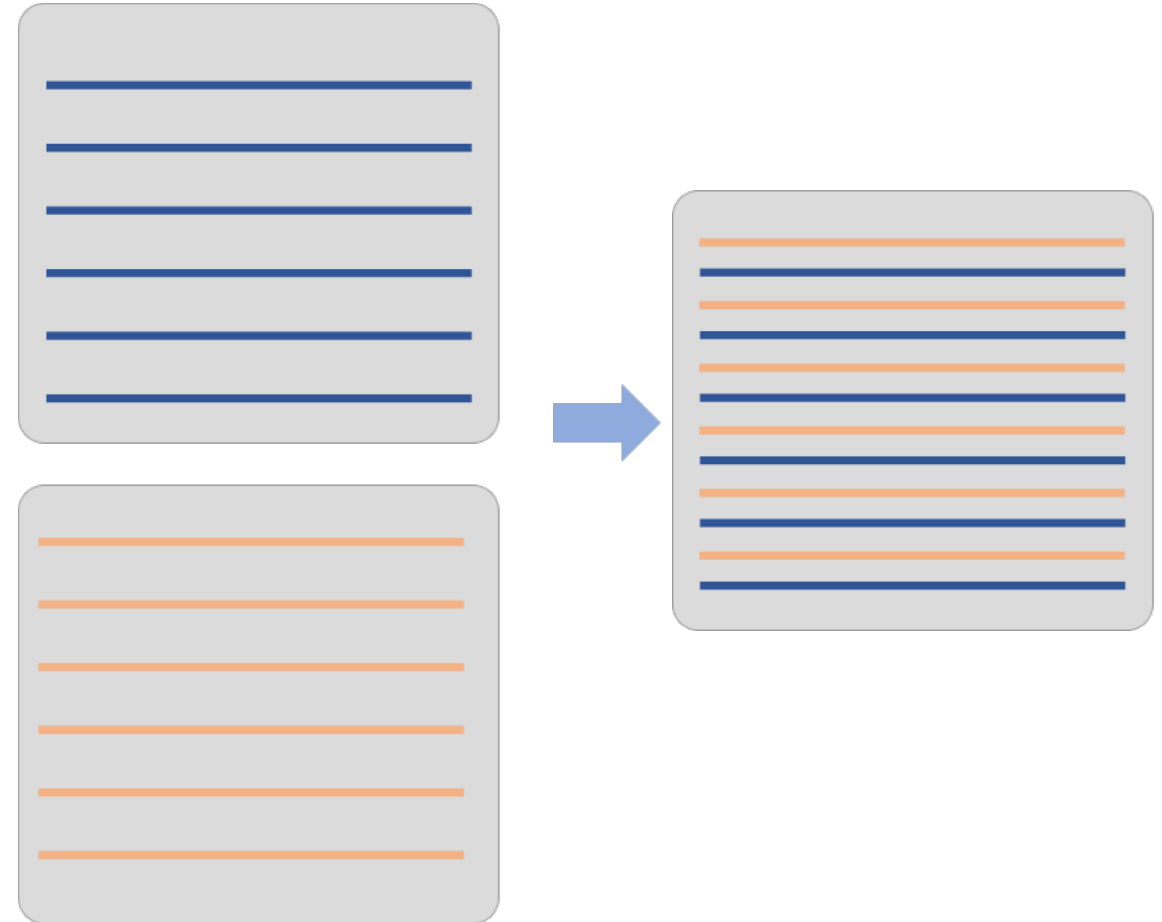
Type of Relationship: Research Support

# Diffusion-weighted imaging

- DWI is sensitive to **molecular motion** and **bulk motion**.
- DWI:  $I(x, y)e^{-bD(x, y)}e^{-i\theta(x, y)}$
- Spatially smooth phase  $e^{-i\theta(x, y)}$  after diffusion encoding
  - Random: because bulk motion is **different** during each application of the diffusion encoding gradients (multi-shot, multi-nex).

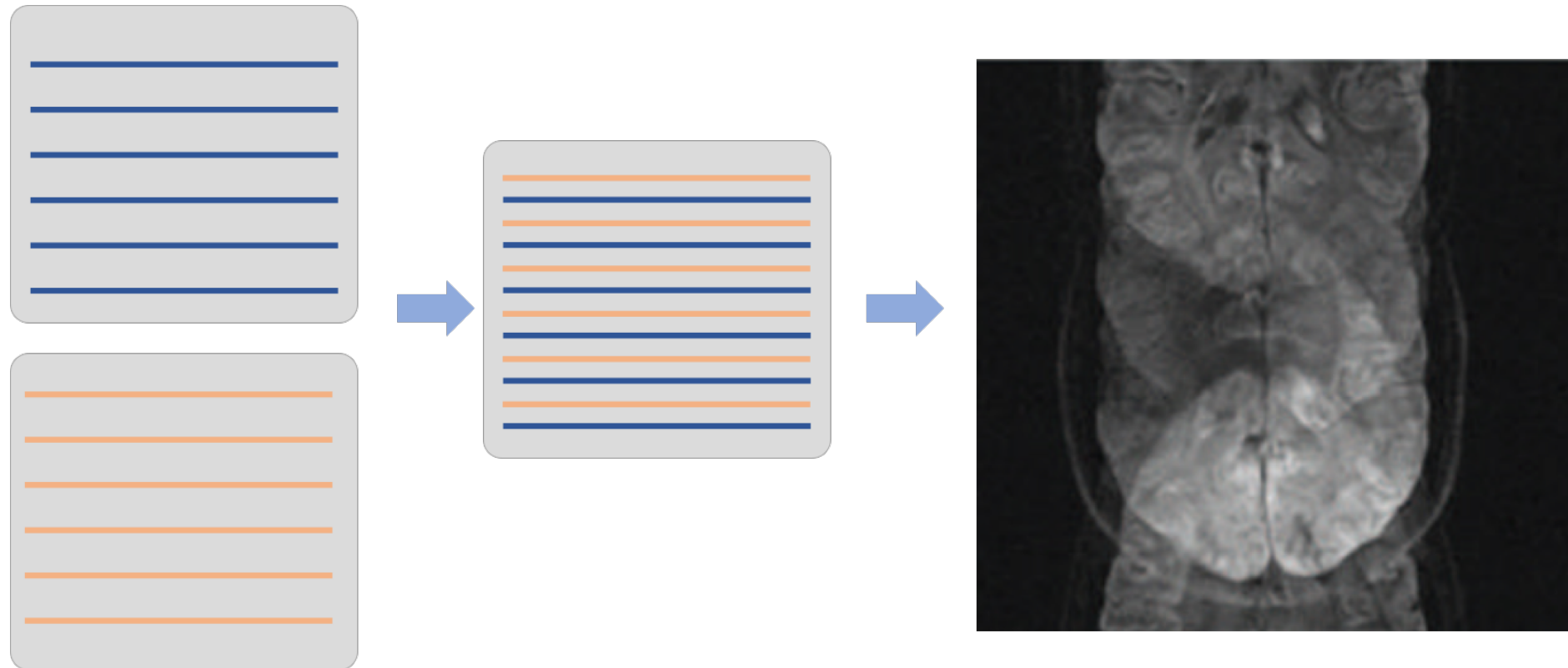
# Diffusion-weighted imaging

- Single-shot imaging (fast)
  - Limited resolution and SNR
  - Heavy distortion
- Multi-shot imaging (slow)
  - Motion sensitive



# Multi-shot DWI

- Higher resolution; reduced distortion.
- Motion-induced phase  $e^{-j\theta(x,y)}$  between shots (random).



# Multi-shot DWI

- Motion-induced phase  $e^{-j\theta(x,y)}$  (random and spatially smooth)
- MUSE/POCS-MUSE

$$\min_{x, \theta_{1, \dots, N_s}} \sum_{i=1}^{N_s} \|D_i F S e^{j\theta_i} x - y_i\|_2^2$$

- Step1: parallel imaging on each shot\*

and take the low-resolution\*\* results to estimate  $e^{j\theta_i}$

- Step2: estimate  $x$

**x**: image to be reconstructed

**$\theta$** : motion-induced phase to be estimated

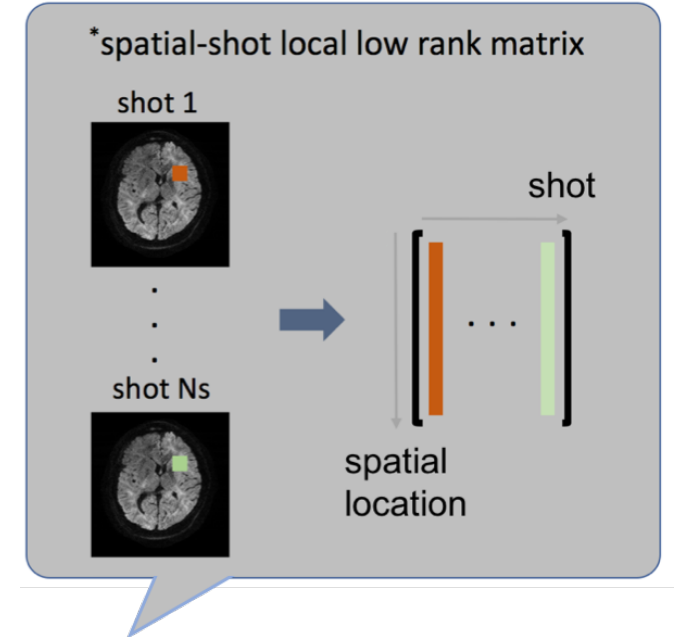
**$D_i$  and  $y_i$** : the sampling operator and  
acquired data of the  $i^{\text{th}}$  shot.

**F**: Fourier transform

**S**: sensitivity map

# Multi-shot DWI

- Motion-induced phase  $e^{-j\theta(x,y)}$  (random and spatially smooth)
- Shot locally low-rank (shot-LLR)
  - “calibration-less parallel imaging”
  - Spatial-shot matrices
  - Slow-phase variations = low-rank



$$\min_{x_1, \dots, x_{N_s}} \sum_{i=1}^{N_s} \|D_i F S x_i - y_i\|_2^2 + \lambda \sum_{b \in \Omega} \|R_b \{x_1, \dots, x_{N_s}\}\|_*$$

Data consistency term

LLR regularization

# Multi-shot DWI

- Motion-induced phase  $e^{-j\theta(x,y)}$  (random and spatially smooth)
- MUSE/POCS-MUSE (non-convex)

$$\min_{x, \theta_1, \dots, \theta_{N_s}} \sum_{i=1}^{N_s} \|D_i F S e^{j\theta_i} x - y_i\|_2^2$$

- Shot locally low-rank (shot-LLR) (**convex**)

$$\min_{x_1, \dots, x_{N_s}} \sum_{i=1}^{N_s} \|D_i F S x_i - y_i\|_2^2 + \lambda \sum_{b \in \Omega} \|R_b\{x_1, \dots, x_{N_s}\}\|_*$$

$\mathbf{x}$ : image to be reconstructed

$\mathbf{x}_i$ : the  $i^{\text{th}}$  shot image to be reconstructed

$\boldsymbol{\theta}$ : motion-induced phase to be estimated

$\mathbf{D}_i$  and  $\mathbf{y}_i$ : the sampling operator and  
acquired data of the  $i^{\text{th}}$  shot.

$\mathbf{F}$ : Fourier transform

$\mathbf{S}$ : sensitivity map



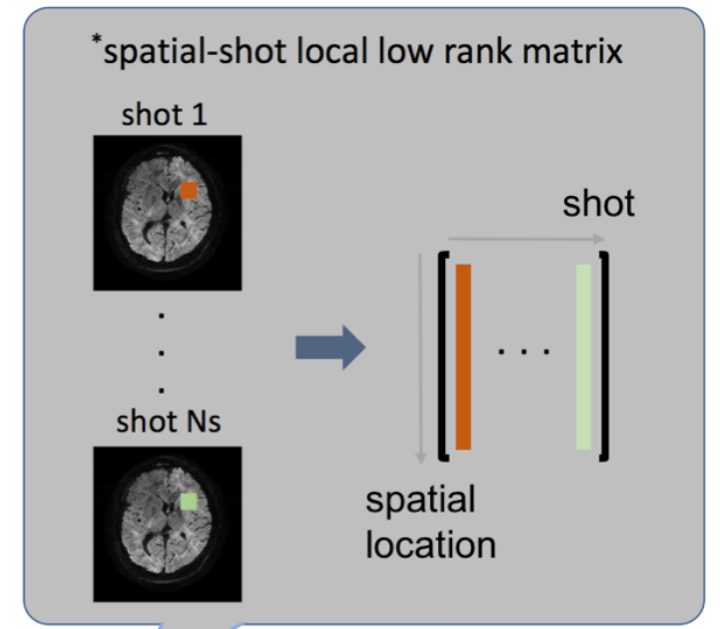
# Multi-shot DWI

- Motion-induced phase  $e^{-j\theta(x,y)}$  (random and spatially smooth)
- MUSE/POCS-MUSE (non-convex)

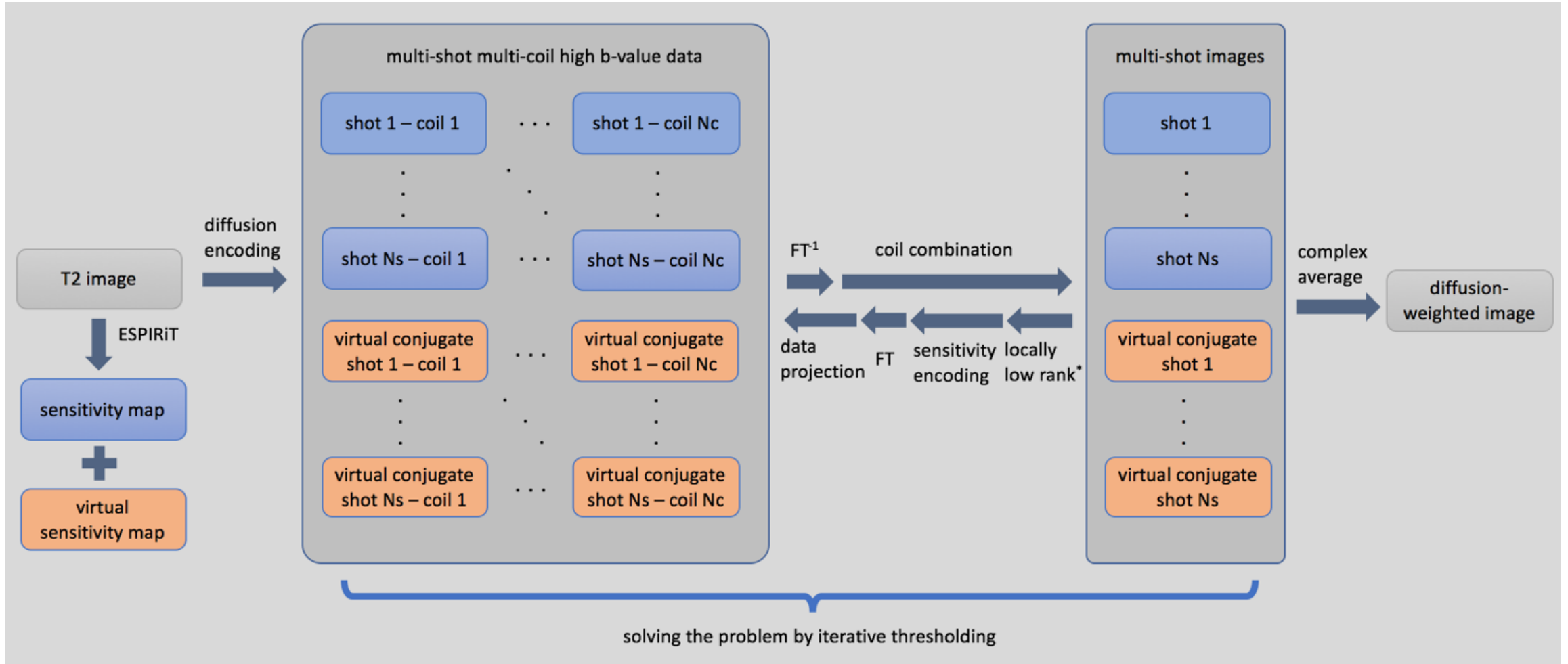
$$\min_{x, \theta_{1, \dots, N_S}} \sum_{i=1}^{N_S} \|D_i F S e^{j\theta_i} x - y_i\|_2^2$$

- Shot locally low-rank (shot-LLR) (**convex**)

$$\min_{x_{1, \dots, N_S}} \sum_{i=1}^{N_S} \|D_i F S x_i - y_i\|_2^2 + \lambda \sum_{b \in \Omega} \|R_b \{x_{1, \dots, N_S}\}\|_*$$



# Flowchart of shot-LLR reconstruction with virtual conjugate shots

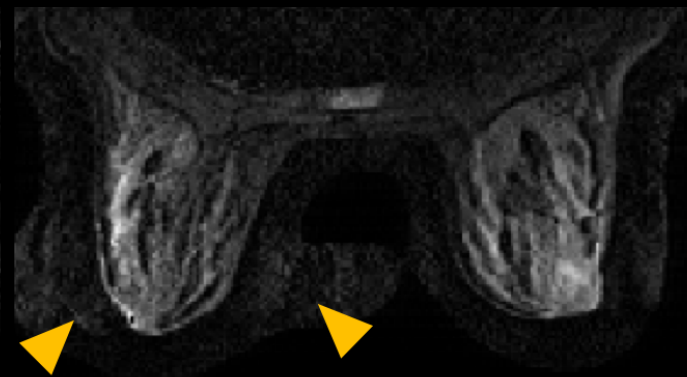
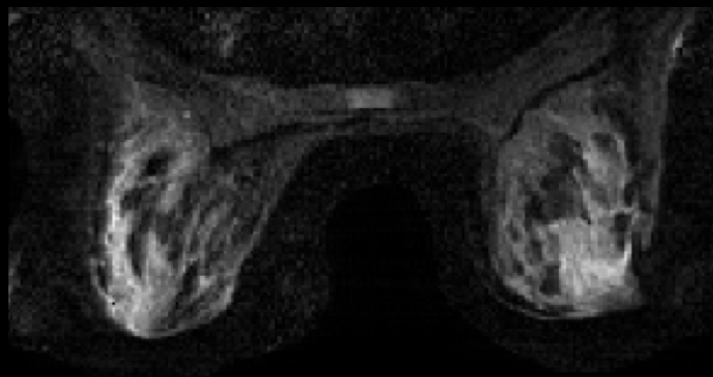


in-plane resolution = 1.44 mm  
slice thickness = 4 mm  
b-value = 600 s/mm<sup>2</sup>

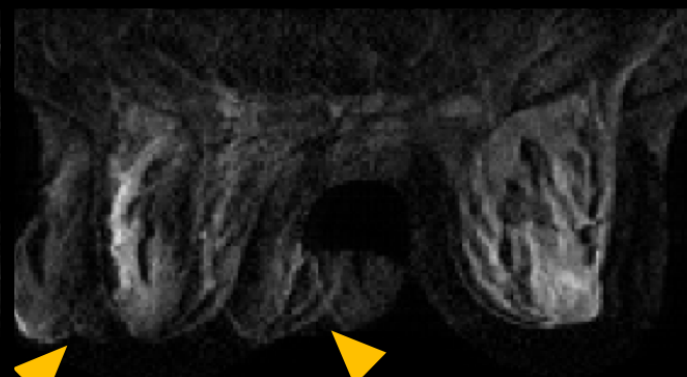
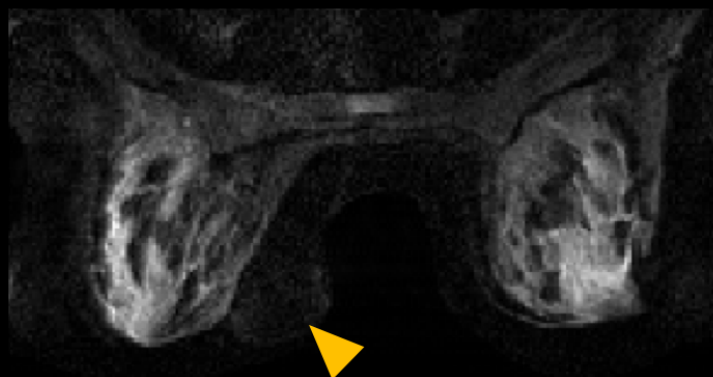
4-shot

8-shot

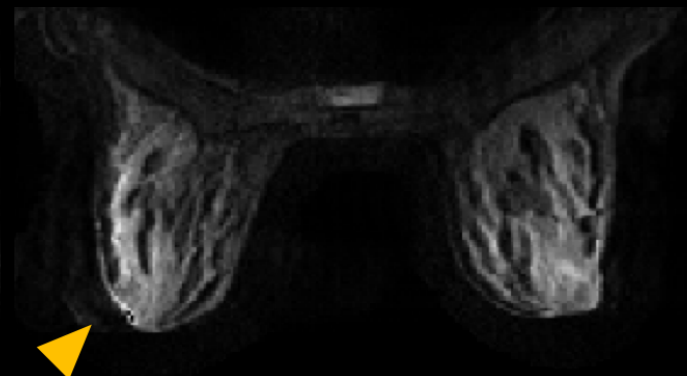
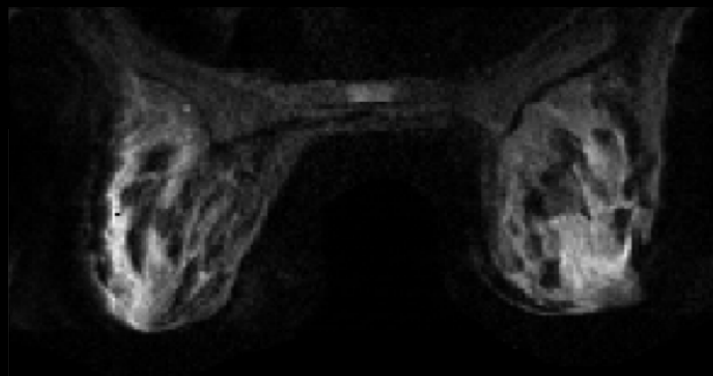
POCS-MUSE



POCS-ICE

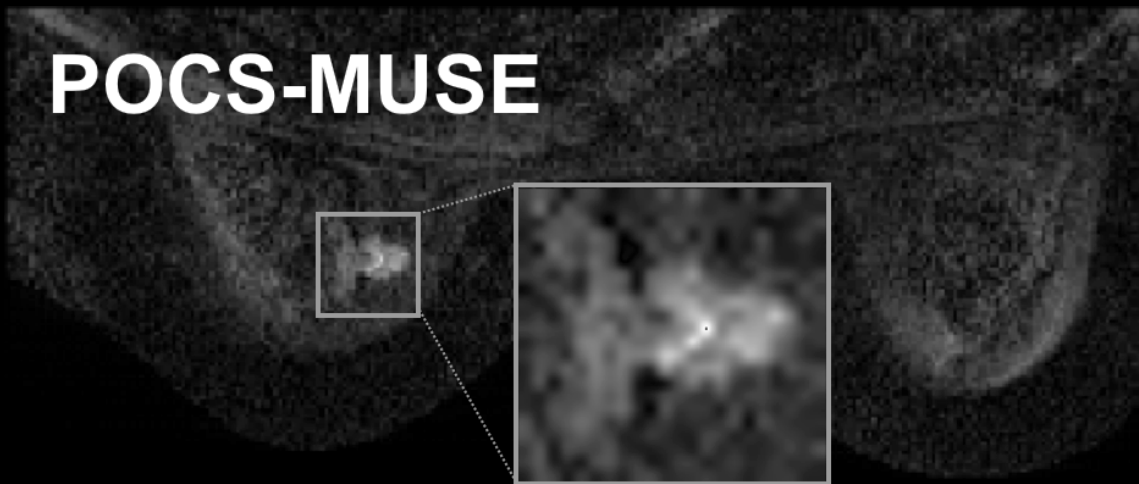


shot-LLR

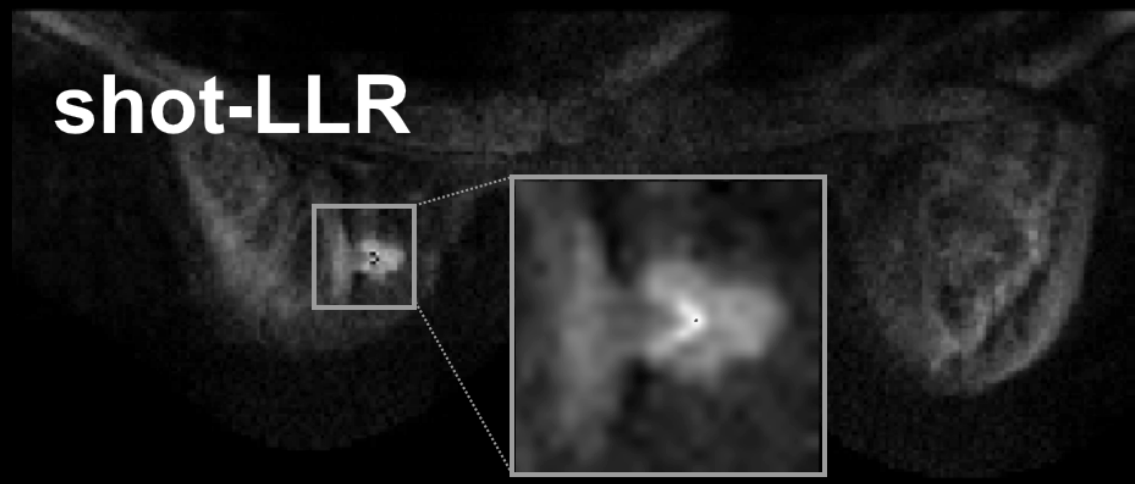


in-plane resolution = 1 mm  
slice thickness = 4 mm  
b-value = 600 s/mm<sup>2</sup>

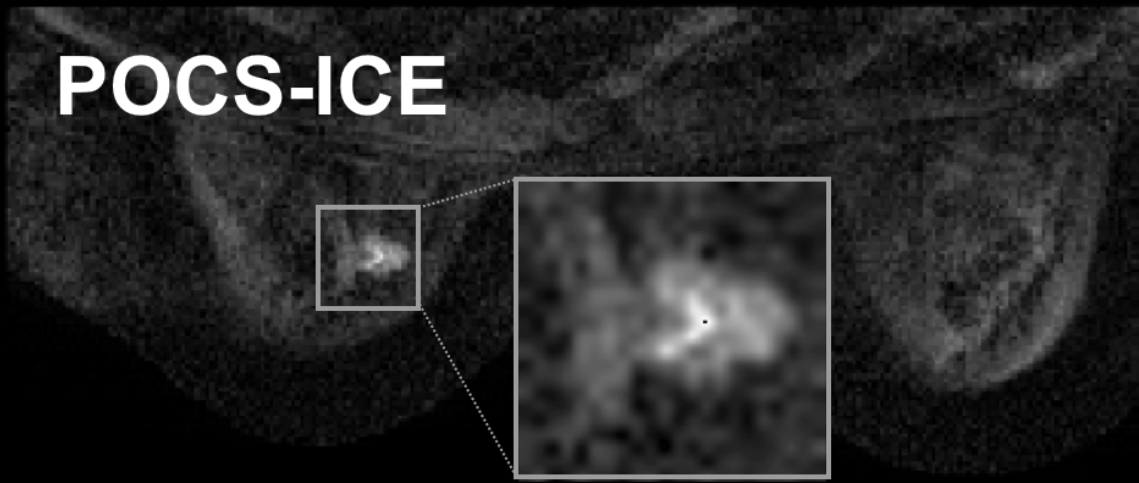
**POCS-MUSE**



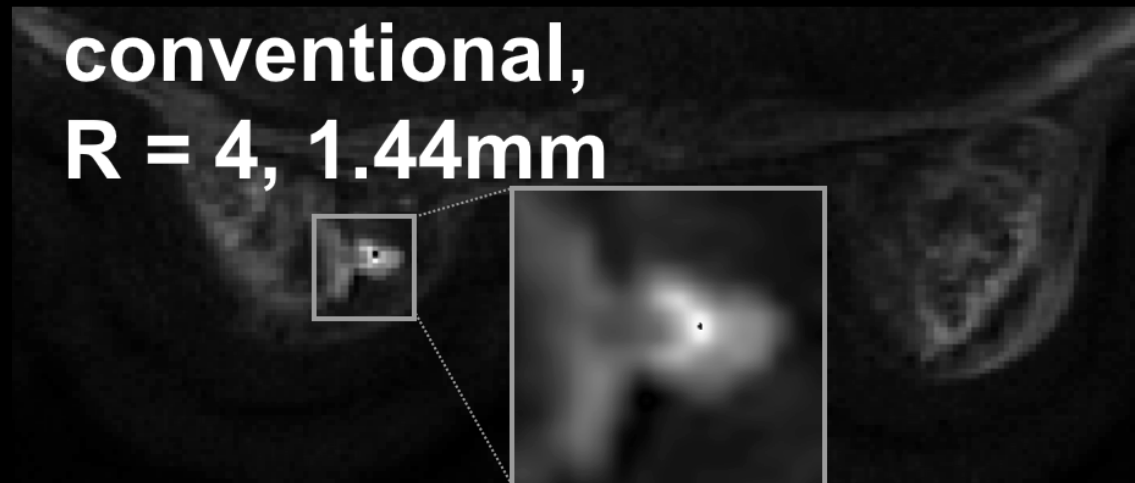
**shot-LLR**



**POCS-ICE**



**conventional,  
R = 4, 1.44mm**



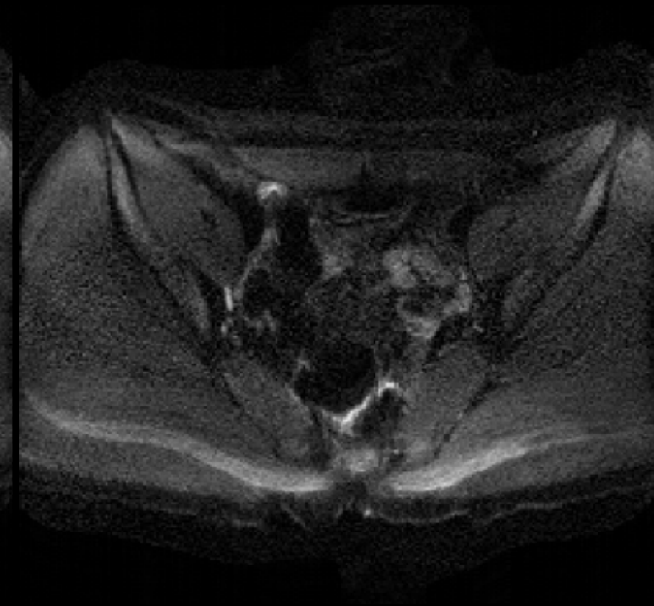
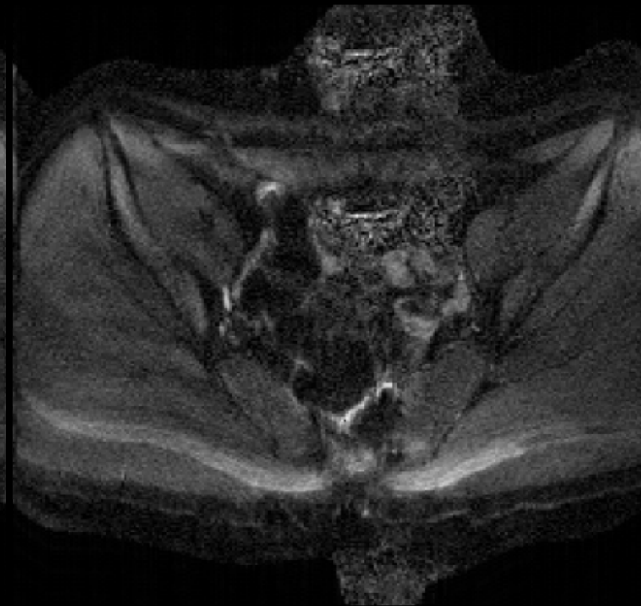
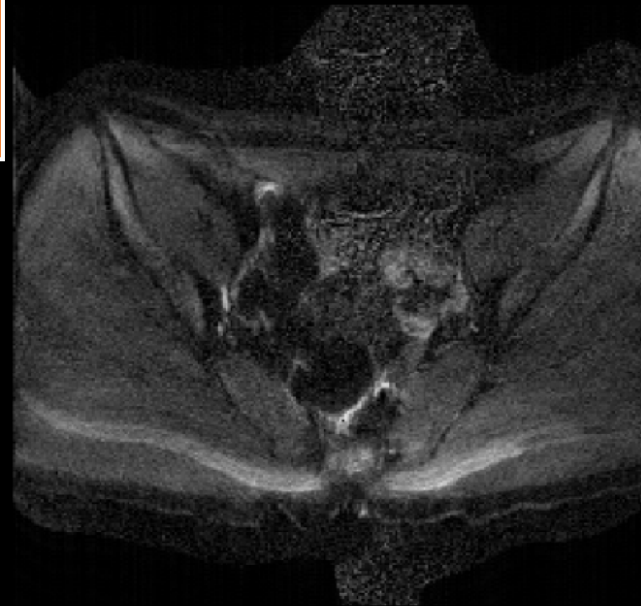
in-plane resolution = 1.1 mm  
slice thickness = 4 mm  
b-value = 500 s/mm<sup>2</sup>

**POCS-MUSE**

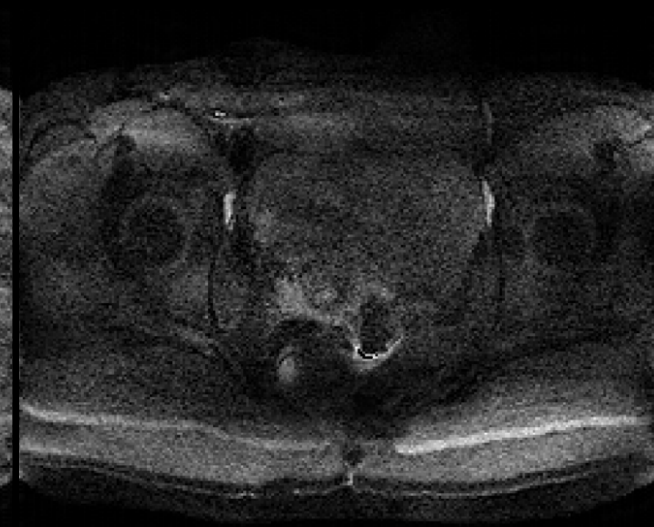
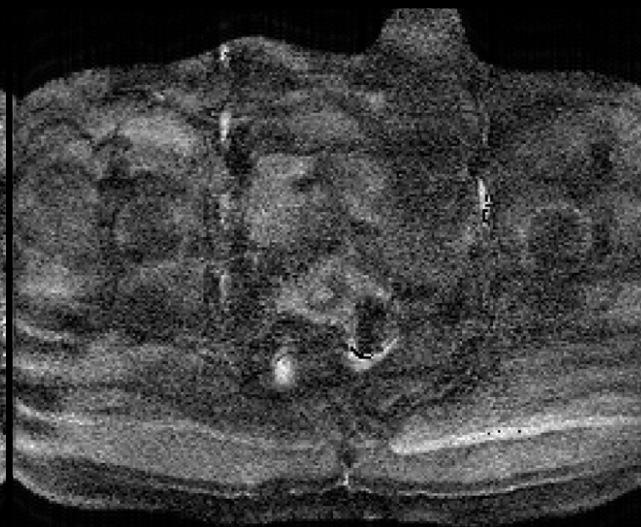
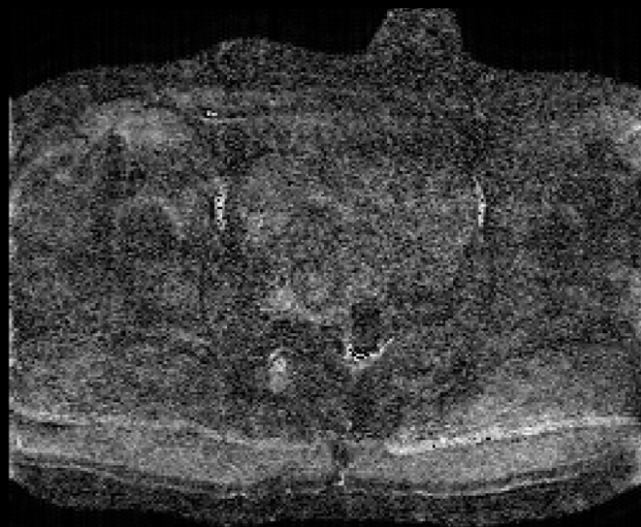
**POCS-ICE**

**shot-LLR**

**4-shot**



**8-shot**



# Summary

## Multi-shot DWI

- Reduced distortion and high resolution
- Shot-to-shot phase variations

## Shot-LLR

- using a relaxed model, non-convex  $\rightarrow$  convex
- constraint on sum of ranks (rank of some matrix can still be high  $\rightarrow$  high frequency phase variations)